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Radiomic assessment of oesophageal adenocarcinoma: a critical review of 18F-FDG PET/CT, PET/MRI and CT



Robert J. O'Shea^{1*}, Chris Rookyard¹, Sam Withey², Gary J. R. Cook^{1,3}, Sophia Tsoka⁴ and Vicky Goh^{1,5}

Abstract

Objectives: Radiomic models present an avenue to improve oesophageal adenocarcinoma assessment through quantitative medical image analysis. However, model selection is complicated by the abundance of available predictors and the uncertainty of their relevance and reproducibility. This analysis reviews recent research to facilitate precedent-based model selection for prospective validation studies.

Methods: This analysis reviews research on 18F-FDG PET/CT, PET/MRI and CT radiomics in oesophageal adenocarcinoma between 2016 and 2021. Model design, testing and reporting are evaluated according to the Transparent Reporting of a Multivariable Prediction Model for Individual Prognosis or Diagnosis (TRIPOD) score and Radiomics Quality Score (RQS). Key results and limitations are analysed to identify opportunities for future research in the area.

Results: Radiomic models of stage and therapeutic response demonstrated discriminative capacity, though clinical applications require greater sensitivity. Although radiomic models predict survival within institutions, generalisability is limited. Few radiomic features have been recommended independently by multiple studies.

Conclusions: Future research must prioritise prospective validation of previously proposed models to further clinical translation.

Keywords: Oesophageal neoplasms, Adenocarcinoma, Prognosis, Machine learning, Precision medicine

Key points

- Radiomic predictor recommendations vary considerably between studies.
- Although radiomic models have demonstrated discriminative predictions in oesophageal cancer tasks, adequate sensitivity has yet to be demonstrated.
- Future radiomic research in oesophageal adenocarcinoma should prioritise validation of previously proposed predictors over further feature selection.

Background

Oesophageal adenocarcinoma presents a major disease burden worldwide, with age-standardised incidence of 0.9 per 100,000 and 1-year survival of 47–55% [1, 2]. Although therapeutic developments have improved survival [2, 3], scope remains to optimise management through improved staging, therapeutic response prediction and prognostication [4–6]. Radiomics—the analysis of quantitative medical imaging features describing morphology, texture and intensity distribution—is a non-invasive method to assess oesophageal adenocarcinomas through quantification of tumour characteristics.

The search for optimal radiomic models is complicated by the breadth of candidate radiomic features and learning algorithms, which present an enormous parameter space to screen. Sample sizes are limited in clinical



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^{*}Correspondence: robert.1.oshea@kcl.ac.uk

¹ Department of Cancer Imaging, School of Biomedical Engineering and Imaging Sciences, King's College London, 5th floor, Becket House, 1 Lambeth Palace Rd, London SE1 7EU, UK Full list of author information is available at the end of the article

imaging studies, creating a scenario in which data-driven feature selection can be unreliable [7–9]. The variation of radiomic feature distributions with imaging equipment, acquisition parameters and annotation methodology presents an additional obstacle for model generalisation [5, 9–11]. Methodological rigour is essential to control false detection rates in such conditions [9], and several reviews have raised concerns regarding design and reporting of imaging models [11–14]. Unsurprisingly, 76% of proposed radiomic predictors are estimated to be false positives [14].

To alleviate biases associated with model selection in individual data sets, studies may validate previously proposed features and models. This approach is a necessary development in the transition from exploration to testing, carrying an appropriate weight in the Radiomics Quality Score (RQS) [15]. However, the complexity of radiomic feature definitions and nomenclature complicate aggregation of results from different studies, hampering validation reproducibility. Accordingly, recent initiatives are now being made in an attempt to standardise radiomic features [15]. This review inspects and evaluates radiomic analyses focussing on the oesophageal adenocarcinoma subtype from a methodological standpoint, extracting features under a unified nomenclature to facilitate future validation studies. The exploratory phase of oesophageal cancer radiomics was well characterised in Van Rossum's 2016 review [16], and here we review subsequent research and developments.

Materials and methods

A literature search was performed to identify original research articles applying radiomics or artificial intelligence to predict stage, therapeutic response or prognosis in human oesophageal adenocarcinoma using PET/ CT, PET/MRI or CT images. Searches were conducted on Embase and MEDLINE databases for full-text articles published in peer-reviewed journals in the English language between 1 January 2016 and 4 January 2022. Search queries are provided in Additional file 1. References of included studies were also screened. Studies with fewer than 10 adenocarcinoma cases, those with squamous cell carcinoma only, and those which omitted histological information were excluded. This threshold reflected the recommended minimum sample size for univariate cox model training [17, 18], whilst avoiding the exclusion of studies with low sample sizes but high quality, such as prospective validation analyses. Where histology-specific results were unavailable, aggregate results were extracted. Studies which modelled both oesophageal and gastroesophageal junction adenocarcinomas were included in this analysis. Transparent Reporting of a Multivariable Prediction Model for Individual Prognosis or Diagnosis (TRIPOD) score [19] and RQS [15] were annotated where applicable. Model validation was classified as "internal", "temporal" or "external" according to whether the data partition represented (1) a random split, (2) a split after a specific time point or (3) a different institution. Radiomic features were extracted and annotated according to Image Biomarker Standardization Initiative nomenclature [20] in the format "Family Feature". A maximum of five features were extracted from each study, according to the most significant associations or model contributions. Radiomic feature selection frequency was estimated for studies analysing primary tumoural radiomics. Visualisation was performed with R, RStudio and ggplot [21–23]. Discrimination performance (e.g. how appropriately a predictor ranks patients with respect to 1-year survival) was quantified by area under the receiver operating characteristic curve (AUC). Categorical associations (e.g. survival time differences between participant groups) were described with χ^2 metrics. Continuous associations (e.g. association of a radiomic feature with volume change) were described with Pearson's correlation (ρ). Cox regression model coefficients (which quantify predictors' contributions a prognostic model) were described by the hazard ratio (HR). Clinical tumour, node and metastasis stages were abbreviated as cT, cN, cM and cTNM; and corresponding post-neoadjuvant pathological stages as ypT, ypN, ypM and ypTNM.

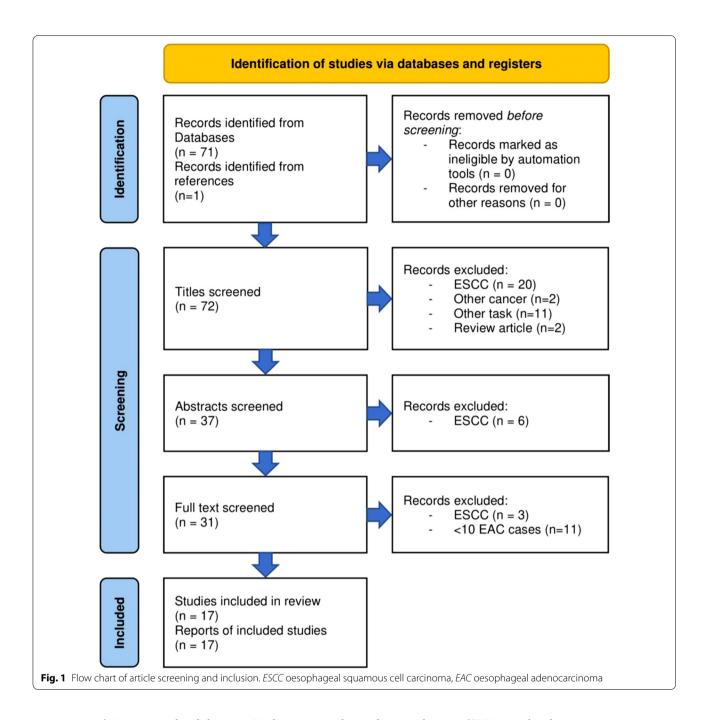
Results

Articles (n=72) were screened and 17 were included in this analysis. A flow diagram of the screening process is provided in Fig. 1 [24]. Article information is summarised in Fig. 2. Results and predictive features from the five studies with the highest RQS are provided in Table 1. Article screening is detailed in Additional file 1: Data S1. TRIPOD annotations are provided in Additional file 1: Data S2. RQS annotations are provided in Additional file 1: Data S3.

Staging 18F-FDG PET

Two 18F-FDG PET studies modelled stage. Zhang modelled ypN on retrospective 18F-FDG PET/CT data from patients receiving chemoradiotherapy (CRT) in two institutions (TRIPOD: 29, RQS: 17) [25]. All 190 patients had adenocarcinoma and underwent neoadjuvant chemoradiotherapy prior to surgery. Supervised feature elimination and L1-penalisation selected four clinical features (age, clinical t-stage (cT), treatment, tumour regression grade (TRG)) and nine radiomic features. PET radiomics added minimal information to clinical features in internal validation (AUC: 0.82 vs. 0.79, p = NR), and the models were equivalent in external validation (AUC: 0.69 vs.

O'Shea et al. Insights into Imaging (2022) 13:104 Page 3 of 12



0.65, p > 0.05). In external validation, cN demonstrated similar discrimination but greater sensitivity, compared with clinical (AUC: 0.66 vs. 0.69, sensitivity: 0.89 vs. 0.52) and clinicoradiomic models (AUC: 0.66 vs. 0.65, sensitivity: 0.89 vs. 0.63).

Baiocco modelled baseline metastatic status retrospectively on prospectively collected serial 18F-FDG PET/MRI data from a single institution (TRIPOD: 24, RQS: 4) [26]. Seventeen out of 20 participants had adenocarcinoma. In training data, a bivariate model of gross tumour

volume radiomics (SUV grey-level co-occurrence matrix (GLCM) GLCM_JointEntropy, ADC GLCM_JointEntropy) demonstrated moderate discrimination (accuracy 0.8, p < 0.001). Adjustments for multiple hypothesis testing were not performed in this exploratory study.

O'Shea et al. Insights into Imaging (2022) 13:104 Page 4 of 12

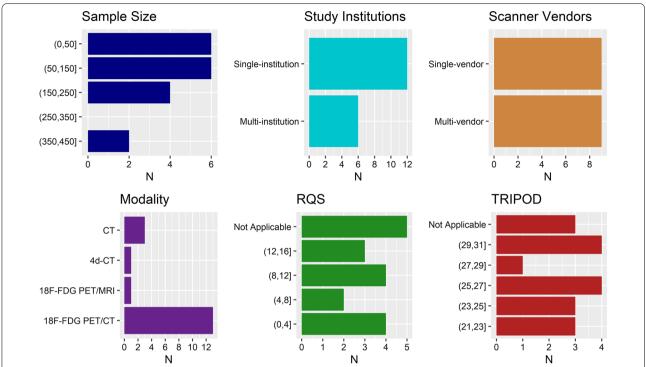


Fig. 2 Histograms of information on included articles. Upper left: study sample size. Upper middle: number of institutions from which data were collected. Upper right: number of scanner vendors with which images were acquired. Lower left: image modality. Lower middle: Radiomics Quality Score (RQS). Lower right: Transparent Reporting of a Multivariable Prediction Model for Individual Prognosis or Diagnosis (TRIPOD) score

Therapeutic response

Summary of studies

18F-FDG PET

Seven studies modelled therapeutic response. Beukinga modelled CRT response on retrospective serial 18F-FDG PET data from patients with locally advanced disease at a single institution (TRIPOD: 27, RQS: 16) [6]. Sixty-three out of 73 patients had adenocarcinoma. Baseline and neoadjuvant radiomic features were evaluated for robustness to segmentation by different annotators. Twelve models were developed with various combinations of clinical and radiomic features. In internal validation, a clinicoradiomic model (cT, post-therapeutic GLCM_AngularSecondMoment) discriminated complete response (TRG=1) better than clinical features (cT, histology) alone (AUC: 0.81 vs. 0.75, p = NR).

In a separate cohort, Beukinga modelled neoadjuvant CRT response on retrospective 18F-FDG PET and genomic data from patients with locally advanced disease at a single institution (TRIPOD: 26, RQS: 14) [27]. Eighty-eight out of 96 patients had adenocarcinoma. Hierarchical clustering was employed to select clinical (cT, histology) and radiomic features (Shape_GearysCMeasure, grey-level run length matrix (GLRLM) GLRLM_LongRunLowGreyLevelEmphasis). In internal

validation, incorporation of gene amplification data (cluster of differentiation 44 and human epidermal growth factor receptor 2 genes) improved clinicoradiomic discrimination of complete response (TRG=1) (AUC: 0.82 vs. 0.69, p=NR). Weaker performance was achieved with clinical features alone (AUC: 0.82 vs. 0.66, p=NR).

Van Rossum modelled CRT response retrospectively on serial 18F-FDG PET data from oesophageal cancer patients at a single institution (TRIPOD: 31, RQS: 12) [4]. Forty-four out of 45 patients had adenocarcinoma. Radiomic feature stability was quantified in a subcohort of 7 patients who had baseline imaging repeated in two institutions. Logistic regression models were generated from clinical (tumour length, cT, therapy, tumour, residual disease on post-CRT biopsy, regression grade) and radiomic features (baseline GLCM_ClusterShade, post-therapeutic metabolic_TumourLesionGlycolysis, post-therapeutic Shape_Sphericity, delta GLRLM_RunPercentage, delta GLCM_JointEntropy). In internal validation, radiomic features improved discrimination of complete (TRG=1) response (AUC: 0.77 vs. 0.72, p = NR). Radiomics were not found to add value at a sensitivity threshold (90%) which could select patients to forego surgery. As the validation set was employed for model optimisation, performance may have been overestimated.

O'Shea et al. Insights into Imaging (2022) 13:104 Page 5 of 12

Table 1 Results and predictive features in the seven studies with the highest RQS and TRIPOD score

Study	Scores	Modality	N	Task	Performance	Radiomic features
[6]	RQS: 16 TRIPOD: 27	18F-FDG PET	73	Response (TRG $= 1$)	Internal: AUC: 0.81	1. GLCM_AngularSecondMoment
[27]	RQS: 14 TRIPOD: 26	18F-FDG PET	96	Response (TRG = 1)	Internal: AUC: 0.82	 Shape_GearysCMeasure GLRLM_LongRunLowGrey LevelEmphasis
[10]	RQS: 13 TRIPOD: 31	18F-FDG PET	403	OS	Internal: χ ₃ ² : 143.14 p < 0.001	 Intensity Histogram_Energy Intensity Histogram_Kurtosis
[43]	RQS: 25 TRIPOD: 31	18F-FDG PET	46	OS	External: χ_3^2 : 1.27 $p = 0.74$	 Intensity Histogram_Energy Intensity Histogram_Kurtosis
[25]	RQS: 17 TRIPOD: 29	18F-FDG PET	190	ypN stage	Internal: AUC: 0.82 95% CI [0.74–0.89] External: AUC: 0.69 95% CI [0.54–0.8]	NGTDM_DependenceEntropy Shape_VolumeDensity NGTDM_Coarseness IntensityHistogram_Minimum HistogramGradient GLCM_InverseDifference MomentNormalised
[25]	"	II	"	OS	External: χ_3^2 : 6.08 p = 0.01	и
[41]	RQS: 12 TRIPOD: 24	СТ	239	OS (3 yr)	Internal: AUC: 0.69 95% CI [0.61–0.77] External: AUC: 0.61 95% CI [0.47–0.75]	1. GLCM_InverseVariance 2. GLDZM_LowGreyLevelZone Emphasis 3. GLRLM_RunLengthNon Uniformity 4. GLCM_InformationMeasure OfCorrelation1 5. NGLDM_DependenceCount Nonuniformity
[4]	RQS: 12 TRIPOD: 31	18F-FDG PET	217	Response (TRG $=$ 1)	<i>Internal:</i> AUC: 0.77 95% CI [0.70–0.83]	GLCM_ClusterShade GLRLM_RunPercentage GLCM_JointEntropy Shape_Sphericity

AUC area under receiver operator characteristic, RQS Radiomics Quality Score, TRIPOD Transparent Reporting of a Multivariable Prediction Model for Individual Prognosis or Diagnosis, TRG tumour regression grade, OS overall survival, ypN post-neoadjuvant nodal status, GLCM grey-level co-occurrence matrix, GLRLM grey-level run length matrix, NGTDM neighbouring grey tone difference matrix, NGLDM neighbouring grey-level dependence matrix

Yip modelled CRT response on retrospective serial 18F-FDG PET data from oesophageal cancer patients at a single institution (TRIPOD: 23, RQS: 3) [28]. Fifty out of 54 patients had adenocarcinoma. Six radiomic features (GLCM_Homogeneity, GLCM_JointEntropy, GLRLM_HighGreyLevelRunEmphasis, GLRLM_ShortRunHighGrayRunEmphasis, grey-level size zone matrix (GLSZM) GLSZM_HighGrayLevelZoneEmphasis, GLSZM_Small-ZoneHighGreyLevelEmphasis) were preselected based on previous studies, and deltas were evaluated. In training data, delta GLCM_JointEntropy discriminated partial response (ypTNM < cTNM) from non-response (AUC: 0.71, p=0.01). However, complete response (ypT=0) was not distinguished. Partitioned model validation was omitted.

Simoni modelled CRT response retrospectively on a prospective 18F-FDG PET data from patients with locally advanced disease at a single institution (TRIPOD: 23, RQS: 3) [29]. Thirty-five out of 53 patients had adenocarcinoma. Radiomic dimensionality reduction was

performed with unsupervised clustering, and five representative features were considered. In training data, two radiomic features (baseline GLCM_JointEntropy and baseline GLCM_InverseDifferenceNormalised) demonstrated univariate associations with response (TRG \leq 2).

CT

Zhang modelled CRT response retrospectively using PET segmentation to support CT radiomic extraction from serial 18F-FDG PET/CT data from a single institution (TRIPOD: 30, RQS: 5) [30]. Although data were sourced from a multicentre trial, patients with images recorded in other institutions were excluded. One hundred fifty-four out of 181 patients (84%) were excluded in total. Nineteen out of 29 included patients had adenocarcinoma. Five radiomic features were preselected based on previous studies. Although adjustment for multiple hypothesis testing was not reported, deltas in three radiomic features (GLCM_InverseDifferenceMoment, GLCM_Contrast, GLCM_Correlation) would have remained

significantly associated with response (ypT $\leq 2)$ under Bonferroni correction. Survival associations (OS ≥ 1 yr) were not identified.

Klaasen modelled chemotherapy response on retrospective serial CT data from stage IVb patients from multiple institutions, extracting radiomic features from hepatic metastases (TRIPOD: 31, RQS: 10) [31]. One hundred ninety-six lesions were included in the analysis. Sixteen out of 18 patients had adenocarcinoma. Patients were restricted to those with visible liver metastases on baseline and post-therapeutic scans. The random forest algorithm was applied to model 370 radiomic features, extracting feature importance according to Gini index. In patient disjoint internal validation, a radiomic model discriminated complete (no residual tumour on second scan) response (AUC: 0.79 [0.74-0.88]). Partial response (>65% volume reduction) was not discriminated as easily (AUC: 0.64 [0.55-0.73]). It is noted that radiomic distributions may differ between primary and metastatic lesions, as was observed by Wagner in a cohort of patients with metastatic colorectal cancer [32].

Outcome discretisation

Where studies discretised continuous variables, valuable information may have been lost [33]. Although TRG is predictive of OS [34], Zhang found no correlation between dichotomised survival (OS>1 yr) and predictors of dichotomised response (ypT \leq 2) [30]. Klaassen dichotomised partial response at 65% volume reduction, according to a computational measurement [31]. Consequently, trivial clinical differences between 64 and 66% tumour volume reduction may have been overrepresented, whilst significant differences between 0 and 64% underrepresented. Indeed, this model learned highly nonlinear decision surfaces—the second most important feature (GLCM_ClusterShade) was perfectly uncorrelated with actual volume decrease (Gini Index: 1.44, Pearson r: 0.0). Furthermore, less important features such as GLCM_InformationMeasureOfCorrelation1, which correlated strongly with volume decrease (Gini Index: 0.81, Pearson r: 0.55) would have yielded informative linear predictors.

Selection bias in therapeutic response studies

Selection biases were apparent in several studies. For example, Beukinga, Zhang and Van Rossum excluded participants with images recorded in other institutions, potentially reducing model generalisability [4, 6, 30]. Klaasen restricted their cohort to patients with visible hepatic metastases on both baseline and post-therapeutic scans [31]. Consequently, the model only observed complete lesion regression in the presence of other visible

disease. The generalisability of these findings to the clinically preferable outcome in which all lesions regress cannot be guaranteed.

Feature preselection

Feature preselection avoids severe adjustments for multiple hypothesis testing, thereby optimising statistical power to detect relevant features within the preselected set. Accordingly, Yip and Foley considered a limited number of radiomic features suggested by previously published results [10, 35-39]. Piazzese and Van Rossum quantified feature stability in subcohorts with images recorded in separate institutions, preselecting features with stable distributions a priori [5, 10]. Although Klaassen preselected feature families based on a previous analysis [40], 370 variables were included in the analysis [31]. Beukinga and Baiocco performed unsupervised feature selection by clustering, conserving power to test a small number of selected variables against the response [26, 27]. Larue and Zhang employed supervised feature selection [25, 41]—this approach retains overfitting risks as the response is observed. Both analyses provided unbiased estimates of model performance through external validation—out-of-sample performance decreases demonstrated overfitting in each case.

Clinical applicability

To inform surgical management decisions, therapeutic response models must demonstrate sensitivity to residual disease, i.e. if watch-and-wait is to be considered following neoadjuvant therapy, models must provide high certainty of complete response. Metrics such as AUC and accuracy may misrepresent performance in this regard. Van Rossum and Yip both identified poor sensitivity to residual disease, highlighting the importance of clinically focussed modelling objectives [4, 28]. Most radiomic models will provide imperfect information—i.e. they improve risk predictions somewhat, but retain relatively high error rates. Such models may be applied more securely in scenarios where the risk-benefit ratios are uncertain, such as in the selection between two therapeutic approaches with similar efficacies. Other potentially valuable applications include therapeutic dose optimisation, as was demonstrated by Her in the optimisation of intensity-modulated radiotherapy for prostate cancer [42].

Survival

Summary of studies

18F-FDG PET

Six studies modelled overall survival (OS). Foley modelled OS on retrospective 18F-FDG PET data from a single institution (TRIPOD: 31, RQS: 13) [10]. Out of 403

participants, 316 had adenocarcinoma. Backwards conditioning was employed to select three clinical features (age, cTNM and treatment intent) and three radiomic features (metabolic_TumourLesionGlycolysis, IntensityHistogram_Energy and IntensityHistogram_Kurtosis) from 19 preselected features. In temporally partitioned validation, clinicoradiomic model quartiles contained more survival information than clinical model quartiles (χ_3^2 : 143.1 vs. 20.6, p=NR).

In a separate study, Foley validated their proposed model on prospective 18F-FDG PET data from three institutions (TRIPOD: 31, RQS: 25) [43]. Thirty-nine out of 46 participants had adenocarcinoma. Neither clinicoradiomic model quartiles nor clinical model quartiles were found to associate with overall survival (χ_3^2 : 1.4 vs. 1.2, p=NR). However, calibration slopes did not differ from unity, supporting preservation of discriminative capacity. Feature harmonisation was also performed with the "combat" algorithm [44], though performance remained similar.

Karahan modelled OS on retrospective 18F-FDG PET data from a single institution (TRIPOD: 23, RQS: 7) [45]. Thirteen out of 62 patients had adenocarcinoma histology. Forty-seven radiomic features were considered. Although several univariate associations were identified between radiomic features and survival outcomes, adjustments for multiple hypothesis testing were not reported—consequently, significance may have been overestimated. Nonetheless, in internal validation, logistic regression models demonstrated good discrimination of 1-year OS (AUC: 0.635) and 5-year OS (AUC: 0.82). Model features were not reported. Analysis was restricted to patients who were known to be alive or deceased at each time interval, resulting in the exclusion of 5/75 patients (7%) lost to follow-up in the first year and 15/75 (20%) lost in 5 years.

Zhang modelled OS in an external cohort using their 18F-FDG PET staging models (TRIPOD: 29, RQS: 17) [25]. The clinicoradiomic model predicted overall survival in the external data (χ_1^2 : 6.08, P = 0.01).

CT

Piazzese modelled OS retrospectively on CT data from a multicentre randomised controlled trial (TRIPOD: 27, RQS: 4) [5]. Fifty-three out of 213 participants had adenocarcinoma, while the majority had squamous cell carcinoma. Radiomic stability was estimated by comparing feature distributions in 2D and 3D images. In a Cox regression model with five clinical features (age, sex, cTNM, WHO performance status, and IV contrast administration) and four stable radiomic features (GLCM_InverseVariance, grey-level distance zone matrix (GLDZM) GLDZM_LargeDistanceEmphasis,

GLDZM_ZoneDistanceNonUniformityNormalised and GLDZM_ZoneDistanceVariance), GLDZM_ZoneDistanceVariance demonstrated significant association with survival (hazard ratio 1.25, $p\!=\!0.03$). Omission of model validation was justified by prioritisation of false positive and negative rates in predictor selection—all observations were used for model fitting.

Larue modelled 3-year OS on retrospective CT data from two institutions (TRIPOD: 24, RQS: 12) [41]. Out of 239 participants, 193 had adenocarcinoma. Recursive feature elimination was employed to select 40 predictors from a set of 1049 radiomic features. The random forest algorithm was employed to model radiomic features (not reported) and clinical features (age, gender, histology, cTNM). Although radiomics outperformed clinical features in internal validation (AUC: 0.69 vs. 0.63, p = NR), similar performance was demonstrated in external validation (AUC: 0.61 vs. 0.62). Supervised feature selection and modelling were performed in separate runs of cross validation, rather than within cross-validation splits. This procedural error is common in radiomic analyses and consequent data leakage results in a bias towards overly complex models [13]. Indeed, decreased external validation performance indicated overfitting.

Selection bias in survival studies

The retrospective time frame of survival analyses may result in various selection biases. Karahan performed two separate exclusions, removing those lost to follow-up at 1 year and 5 years, respectively. Consequently, participants lost to follow-up due to death were excluded from survival outcomes, inducing bias [46]. Larue excluded cases which did not undergo surgery, although this information would not be available for the immediate application of a pre-treatment imaging model [41]. Piazzese utilised trial data, and exclusions were not reported [5]. Foley's exclusions were most suited to clinical application, as they were clearly described and based on contemporaneous variables with research precedent (SUV_{max} < 3, MTV<5 ml, histology other than adenocarcinoma or squamous cell carcinoma, synchronous malignancies and oesophageal stenting) [10, 43]. Foley's validation study provided the most unbiased estimates of model performance, as the model and exclusions were fixed prior to application in a prospective data set [43].

Clinical applicability

As the clinical consequences of false positives and false negatives rarely equate, traditional model metrics may have limited relevance at patient level and further decision curve analysis may be required [4]. Larue found that their model demonstrated a 24% false negative rate for 3-year mortality, concluding that the model cannot

support treatment decisions [41]. Beyond use for management decisions, radiomic survival models may find an important application in patient information. Oncology patients rank life expectancy as their highest information priority [47]. Consequently, an additional objective risk measure may improve patient-centred care if used appropriately. However, radiomic models' complexity and reliability may prove difficult to communicate in practice.

Evaluation of technical aspects Stability of radiomic features

18F-FDG PET

Whybra [48] assessed radiomic feature robustness to resampling on retrospective 18F-FDG PET data from patients at a single institution (RQS: 3). Nineteen out of 131 patients had adenocarcinoma. Radiomic distributions were found to vary with interpolation method.

Van Rossum et al. [4] evaluated feature stability in a subset of their cohort with baseline 18F-FDG PET images recorded in both the institutions. Both segmentations were performed by a single clinician. Shape and metabolic features demonstrated high stability; first-order, GLCM and GLRLM features demonstrated moderate stability; and neighbouring grey tone distance matrix (NGTDM) features demonstrated poor stability.

CT

Larue [40] evaluated stability of radiomic features with respect to respiratory phase in 4D-CT data from patients at a single institution. Twenty out of 40 had adenocarcinoma. Wavelet filtered image features were found to be less robust than features computed on the original image. Shape features and GLDZM features were the most stable feature families overall.

Impact of segmentation methods

Parkinson [49] evaluated the impact of segmentation methodology on survival models developed in Foley's cohort [10] (TRIPOD: 27, RQS: 11). Six segmentation algorithms were applied. Radiomic features varied to the extent that some survival associations reversed.

Yip [35] modelled therapeutic response in retrospective serial 18F-FDG PET data from a single centre, evaluating the impact of contour propagation methodology (RQS: 3). Forty-four out of 45 patients had adenocarcinoma histology. Three preselected features' deltas (GLCM_JointEntropy, GLRLM_ShortRunHighGreyRunEmphasis, GLZSM_ShortZoneHighGreyLevelEmphasis) were found to be robust to registration algorithm variation.

Radiomic features' volume dependence

Several studies identified associations between observed radiomic features and tumour volume [35, 49]. Following

Hatt's recommendations [50], Van Rossum and Foley excluded small tumours from their analyses [4, 25]. Volume confounding may be evaluated by inclusion of volume as a predictor [50]. Several studies also noted the limitation that radiomic features may vary according to segmentation method [10, 28, 31, 45].

Radiomic feature selection frequency

The feature space of radiomic models varied considerably between studies. Disregarding image transformations, 21/25 identified features were recommended by one study each. The most frequently selected feature was GLCM_JointEntropy, appearing in five PET studies [4, 28–30, 35] and one CT study [30]. A histogram of radiomic feature selection frequency is provided in Fig. 3. Significant radiomic features extracted from each article are provided in Additional file 1: Data S4.

Discussion

Summary of findings

Although staging models demonstrated discriminative capacity [25, 26], sensitivity afforded by radiologists was unmatched. Radiomic models of therapeutic response demonstrated marginally higher discrimination than clinical models in three studies [4, 6, 27]. However, radiomic features did not improve clinical models' sensitivity to residual disease where evaluated [4, 28]. Survival models were informative; however, generalisability was limited [5, 10, 41, 43, 45].

Design and reporting standards

Many studies followed design and reporting recommendations—Foley followed Moons' biomarker development recommendations [10, 43, 51] and Klaasen, Larue, Van Rossum, Piazzese and Zhang cited TRIPOD guidance [4, 5, 25, 41]. TRIPOD scores ranged from 23/31 to 31/31, indicating comprehensive reporting. TRIPOD compliance enhanced transparency and reproducibility. However, RQS ranged from 3/36 to 25/36 with a median score of 11/36, highlighting many opportunities for design improvement from a radiomics perspective. In particular, only one prospective validation study was identified [43]. These findings concur with previous analyses [11, 12, 52, 53].

Modelling algorithms

Minimally complex models such as logistic regression, linear discriminant analysis and cox regression were employed in most studies [4–6, 10, 25, 27, 30, 45, 49]. The small parameter spaces of these algorithms suited the limited sample sizes available, particularly where full sets of radiomic predictors were considered. Regression-based models are also amenable to biological

O'Shea et al. Insights into Imaging (2022) 13:104 Page 9 of 12

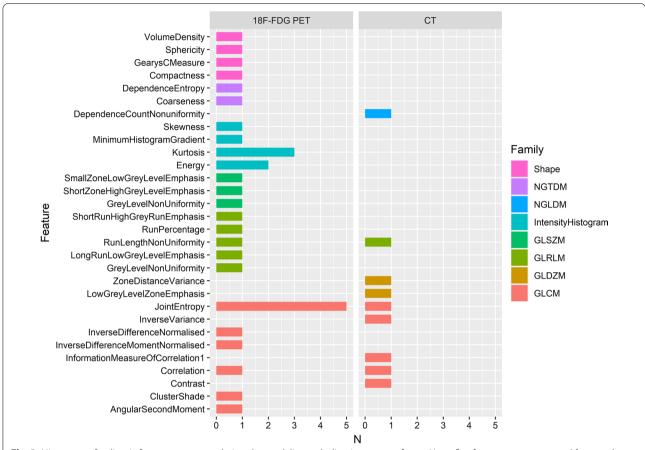


Fig. 3 Histogram of radiomic feature recommendations by modality, excluding image transforms. Up to five features were extracted from each study, according to significance or model contribution. *GLCM* grey-level co-occurrence matrix, *GLDZM* grey-level distance-zone matrix, *GLRLM* grey-level run length matrix, *GLSZM* grey-level size zone matrix, *NGTDM* neighbouring grey tone difference matrix, *NGLDM* neighbouring grey-level dependence matrix

interpretation as coefficients describe the direction and magnitude of the estimated effects. Klaasen and Larue [31, 41] developed random forest models. The instability of importance measures in the high-dimensional setting [54] complicates application of random forest modelling to radiomic feature selection—this approach is best applied to data sets where observations outnumber variables [9]. Indeed, Larue's model demonstrated decreased performance in external validation [41]. Furthermore, random forest decision functions require complex descriptions, impending reproduction.

External validation and generalisability

Radiomic feature distributions may differ between centres, due to variability in scanner model, acquisition parameters and population characteristics [6, 10, 25, 27, 31, 45], prompting calls for standardisation of these parameters [27, 41, 45]. Accordingly, Piazzese, Beukinga and Karahan preselected features on the basis of stability [5, 6, 45]. Both studies testing inter-institutional

generalisability demonstrated performance decreases [25, 41], indicating that some degree of overfitting occurred. Lack of external validation was frequently cited as a limitation [6, 25, 27, 29–31, 41]. Of five studies which performed internal validation, only Foley reported the performance of a single finalised model on test data which was unobserved during training or model selection [10]. Although Foley did not find their model performance significant in external validation, it should be noted that the small sample size of the external data set limited the power to detect significant results [43].

Study limitations

Recognising the distinct clinical prognostic profiles of oesophageal adenocarcinoma and squamous cell carcinoma [2], the studies analysed in this review were selected to provide a large predominance of adenocarcinomas. However, the inability to completely separate the small amount of squamous cell carcinoma data in some included studies may reduce specificity of the feature

O'Shea et al. Insights into Imaging

(2022) 13:104

recommendations for a pure adenocarcinoma cohort. Comparison of individual study findings was also complicated by variability in the considered features, selection methods and modelling algorithms. Furthermore, statistical measures of association varied, precluding conventional meta-analysis. Comparative evaluation of image modalities was further precluded due to the paucity of studies evaluating CT and MRI. Our study reports frequency of feature selection, ignoring significance and direction of effect in individual studies. Inclusion of small studies allowed for faithful representation of the diverse conditions across different studies—however, greater feature selection variability and lower feature significance may be expected in smaller studies. Finally, this analysis was limited to studies published in the English language.

Conclusions

Radiomic models for 18F-FDG PET, MRI and CT have been proposed for staging, therapeutic response assessment and prognostication. Many studies have reported significant results. An urgent clinical need exists for a generalisable, rigorously tested prognostic model for oesophageal adenocarcinoma. Thus, future studies must prioritise unbiased model validation over further exploratory research. This review consolidates study findings and proposes features to facilitate precedent-based design of prospective radiomic studies.

Abbreviations

AUC: Area under receiver operator characteristic; CRT: Chemoradiotherapy; cTNM, cT, cN, cM: Clinical tumour node metastasis stage; GLCM: Grey-level co-occurrence matrix; GLRLM: Grey-level run length matrix; GLSZM: Grey-level size zone matrix; HR: Hazard ratio; NGLDM: Neighbouring grey-level dependence matrix; NGTDM: Neighbouring grey tone difference matrix; NR: Not reported; OS: Overall survival; PFS: Progression-free survival; RQS: Radiomics Quality Score; TRG: Tumour regression grade; TRIPOD: Transparent Reporting of a Multivariable Prediction Model for Individual Prognosis or Diagnosis; ypTNM, ypT, ypN, ypM: Post-neoadjuvant pathological tumour node metastasis stage; ρ : Pearson's correlation coefficient; χ^2_k : Chi-squared statistic with k degrees of freedom.

Supplementary Information

The online version contains supplementary material available at https://doi.org/10.1186/s13244-022-01245-0.

Additional file 1: S1. Details of all screened articles.**S2.** Tripod scores of included articles.**S3.** Radiomic quality scores of screened articles. **S4.** Significant radiomic features in included articles.

Author contributions

All authors contributed to the study conception and design. Material preparation, data collection and analysis were performed by RO'S. The first draft of the manuscript was written by RO'S, and all authors commented on previous versions of the manuscript. All authors read and approved the final manuscript.

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Availability of data and materials

All studies included in this analysis are available from their relevant publications. Search queries are provided in Additional file 1. Article screening is detailed in Additional file 1: Data S1. TRIPOD annotations are provided in Additional file 1: Data S2. RQS annotations are provided in Additional file 1: Data S3. Significant radiomic features extracted from each article are provided in Additional file 1: Data S4.

Declarations

Ethics approval and consent to participate

Not applicable.

Consent for publication

Not applicable.

Competing interests

The authors of this manuscript declare no relationships with any companies, whose products or services may be related to the subject matter of the article.

Author details

¹Department of Cancer Imaging, School of Biomedical Engineering and Imaging Sciences, King's College London, 5th floor, Becket House, 1 Lambeth Palace Rd, London SE1 7EU, UK. ²Department of Radiology, The Royal Marsden NHS Foundation Trust, London, UK. ³King's College London & Guy's and St Thomas' PET Centre, St Thomas' Hospital, London, UK. ⁴Department of Informatics, School of Natural and Mathematical Sciences, King's College London, London, UK. ⁵Department of Radiology, Guy's and St Thomas' NHS Foundation Trust, London, UK.

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